

Reviews

Dose-dependent Pharmacokinetics and Cancer Chemotherapy

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Summary. *Dose-dependent pharmacokinetics have been reported more frequently for anticancer drugs than for other drugs, probably because anticancer drugs are studied over a wide range of doses during early evaluation and because of the increasing use of anticancer drugs at very high doses. Dose-dependent pharmacokinetics are reflected most commonly as an increase in the biological half-life of a drug and a greater than proportional increase in plasma concentration of the drug and in area under the drug concentration-time curve with increase in dose. Occasionally the rate of drug removal increases with increasing dose. These nonlinear changes in drug concentrations with dose may lead to increases in toxicity out of proportion to increases in dose. Appreciation of the possibility of dose-dependent pharmacokinetics is important in the clinical pharmacologic evaluation of new drugs, and may be essential for the design of effective therapeutic regimens.*

Elimination of most drugs from the body typically follows first-order kinetics, and pharmacokinetic parameters describing elimination of a drug do not change over the therapeutic dose range. A limited number of drugs exhibit dose-dependent pharmacokinetics (also called nonlinear pharmacokinetics), where pharmacokinetic parameters depend upon the dose of drug employed. In some cases pharmacokinetic parameters may change during elimination of a single dose of drug as a function of drug concentration in the body. The theoretical basis for dose-dependent pharmacokinetics has received extensive treatment [48, 69, 75, 113]. This report reviews major types of dose-dependent pharmacokinetics and specifically addresses dose-dependent pharmacokinetic behavior of anticancer drugs in humans.

Types of Dose-dependent Pharmacokinetics

A major cause of dose-dependent pharmacokinetics is saturation of the capacity of an enzyme or carrier system for drug biotransformation or excretion. The kinetics of these processes can often be described by the Michaelis-Menten equation:

$$\frac{-dC}{dt} = \frac{V_m C}{K_m + C};$$

where $-dC/dt$ is the rate of decline of drug concentration C , at time t , V_m is the theoretical maximum rate of the process, and K_m is the Michaelis constant. When C is greater than K_m , the rate of the reaction approaches V_m and is independent of the plasma concentration of the drug (that is, a zero-order process). As the concentration falls and C becomes considerably smaller than K_m , elimination becomes first-order. Elimination of drug at high doses is characterized initially by a zero-order process followed by first-order elimination as the concentration falls. At lower doses only first-order elimination is observed. The first-order rate constant and $t_{1/2}\beta$ (the biologic half-life) is the same at all doses. The T50% (time to eliminate 50% of the dose), however, increases with dose. Drugs whose biotransformation becomes capacity-limited at high doses in humans include ethanol [78], salicylate [74], diphenylhydantoin [3, 46, 57], sulfamethazine [32, 86], and possibly propranolol [39]. Dose-dependent pharmacokinetics of propranolol have not been found by all workers [50]. Capacity-limited renal tubular excretion may be responsible for dose-dependent pharmacokinetic behavior of chlorthalidone [41] and piperacillin [6]. Saturation of biliary excretion has been implicated in the dose-dependent pharmacokinetic behavior of rifampicin [1].

The pharmacokinetic consequences of plasma protein binding of drugs has received considerable

attention [19, 70, 79, 100]. If drug elimination is principally a function of free (unbound) drug concentration, then as the capacity of plasma proteins to bind drug is saturated at high drug concentrations, the plasma concentration of free drug and the rate of drug elimination increase. In general, because of the increased rate of elimination of free drug, as the dose of drug is increased the plasma concentration of total drug and the area under the concentration-time curve (AUC) do not exceed a constant (plateau) value. This phenomenon has been observed for several drugs that bind extensively to plasma proteins, such as phenylbutazone [12], naproxen [99], and disopyramide [28, 80]. It should be emphasized that concentration-dependent binding of a drug to plasma proteins over the therapeutic range does not necessarily lead to dose-dependent pharmacokinetics. For example, the binding of lidocaine to plasma proteins is dose-dependent over the range of therapeutic plasma concentrations. Despite this, lidocaine does not show dose-dependent plasma elimination because both free and protein-bound lidocaine are efficiently metabolized by the liver [80].

Binding of drug to tissue proteins can result in dose-dependent pharmacokinetic behavior similar to that for drugs that bind to plasma proteins provided the capacity of tissue binding sites is saturated over the therapeutic range. Prednisolone exhibits an increase in the apparent volume of distribution (V_d) as the dose is increased [90, 98, 108] without a concomitant change in plasma protein binding [108]. Increased binding to tissues with increasing dose has been proposed to account for this dose-dependent effect on the V_d of prednisolone [98, 108].

Absorption is another factor that might influence the pharmacokinetics of an orally administered drug. It has been suggested that a dose-dependent decrease in the rate of absorption contributes to the nonlinear pharmacokinetics of sulfamethazine [32].

Dose-dependent pharmacokinetics may result when a metabolite inhibits processes responsible for biotransformation of parent drug. This occurs when a slowly eliminated metabolite capable of inhibiting an enzyme that metabolizes the parent compound reaches inhibitory concentrations at a time when the concentration of the parent drug is lower than its K_m for the enzyme. Theoretical aspects of product inhibition on the kinetics of drug elimination have been reviewed by Perrier et al. [89]. An intriguing aspect of product inhibition is that drug concentrations decline more slowly over a given range of concentrations following a high dose of drug than following a low dose of drug. Drug elimination appears to be first-order and $t_{1/2\beta}$ increases with increasing dose. This phenomenon has been termed

the dose-dependent 'memory' effect. It has been suggested [4, 48] that this type of dose dependency is seen in humans following administration of dicoumarol [87] and diphenylhydantoin [3].

Several drugs show dose-dependent pharmacokinetics in humans, mediated by mechanisms which have not been established with certainty. These include heparin [10], theophylline [67, 115], disopyramide [60], carbamazepine [9], and chloroquine [42]. Chronic administration of chloroquinone produces remarkable changes in pharmacokinetic parameters. As the dose is increased from 250 to 1,000 $\text{mg} \cdot \text{kg}^{-1} \cdot \text{day}^{-1}$ there is an increase in $t_{1/2\beta}$ from 3–312 min, and a 1,000-fold increase in the AUC normalized for dose.

Dose-dependent Pharmacokinetics of Anticancer Drugs

In initial human studies anticancer drugs are frequently administered over a wide range of doses. It is not surprising that dose-dependent pharmacokinetic behavior has been noted for many anticancer drugs. Dose-dependent pharmacokinetics is suggested when the plasma concentration of drug or AUC does not vary linearly with dose and when the fraction of drug or metabolites excreted in the urine over time varies with dose.

High-dose Cancer Chemotherapy

Some anticancer drugs are administered at doses sufficiently large to saturate processes with limited capacity, such as metabolism and renal tubular secretion. Methotrexate is conventionally administered at doses of about 30 mg/m^2 . When therapy is followed by 'rescue' courses of leucovorin, methotrexate has been given at doses up to 12 g/m^2 . High-dose methotrexate has been reported to exhibit dose-dependent pharmacokinetics characterized by increasing apparent initial volume of distribution and decreasing urinary clearance with increasing dose [73, 96]. Over 90% of IV administered methotrexate is excreted in the urine unchanged [59, 64, 94, 114]. It has been suggested that methotrexate is filtered at the glomerulus and actively secreted by renal tubular cells [11]. Reich [95] has recently developed an operational pharmacokinetic model incorporating renal tubular secretion with Michaelis-Menten kinetics for high-dose methotrexate infusion. The apparent K_m obtained by curve-fitting the plasma concentrations of methotrexate in three patients receiving a 24-h infusion of methotrexate in doses between 1.5

and 4 g/m^2 was $5 \times 10^{-5} \text{ M}$ to 10^{-4} M . On the basis of these data, dose-dependent pharmacokinetics would not be expected until plasma methotrexate concentrations exceed 10^{-4} M . Concentrations greater than 10^{-4} M are achieved in patients with normal renal function at doses of methotrexate greater than 5 g/m^2 given over 24 h [58, 95], and concentrations in excess of 10^{-3} M are attained when large doses of methotrexate are given rapidly [20, 61, 105]. Monjanel et al. [81] have used a linear pharmacokinetic model to predict plasma concentrations of methotrexate in patients receiving 1.5 g/m^2 over 36 h (plasma levels of about 10^{-5} M), with apparent success. Goh et al. [49] studied children receiving methotrexate at a dose of $25\text{--}150 \text{ mg/kg}$ ($0.45\text{--}4.5 \text{ g/m}^2$) by 24-h infusion. Their results show more rapid elimination of methotrexate at serum concentrations greater than 10^{-4} M . Not all studies have found dose-dependent pharmacokinetics after high-dose methotrexate therapy. Pratt et al. [94] gave children methotrexate at $100\text{--}500 \text{ mg/kg}$ over 6 h and reported serum levels up to 10^{-3} M . There was, however, no change in the half-life of the elimination of drug from serum with increase in dose, and they concluded that the capacity for clearing methotrexate from blood was not saturated at these doses. The mean half-life, 157 min, observed by Pratt et al. [94], was similar to the half-life reported by others at much lower doses of methotrexate, 134 min at a dose of 10 mg/kg [55] and 210 min at 30 mg/m^2 [59]. Stoller et al. [105] reported a similar initial half-life of 126 min after methotrexate administration at $50\text{--}200 \text{ mg/kg}$ over 6 h.

Thymidine has been administered in high doses up to 128 g/m^2 over 24 h [35], achieving millimolar plasma concentrations [17, 117]. At these concentrations, thymidine has been reported to have a selective cytotoxic effect on tumor cells [72]. Thymidine is eliminated by metabolism, renal glomerular filtration, and renal tubular secretion [117]. Metabolism and renal secretion are saturated at high doses. At lower doses of thymidine, 8 g/m^2 over 24 h, the half-life of plasma thymidine after cessation of infusion was 10 min. The calculated total-body clearance was $16.0 \text{ l/min per m}^2$, and less than 2% of the total dose was excreted in the urine as unchanged thymidine [34]. At high doses, 75 g/m^2 over 24 h, the half-life was 100 min. Total-body clearance was $0.1 \text{ l/min per m}^2$, and only 39% of the dose was removed by metabolism [17, 117]. Woodcock et al. [116] have studied the pharmacokinetics of thymidine in humans receiving a fixed dose of 5-fluorouracil preceded by increasingly large doses of thymidine given by rapid infusion. As the dose of thymidine was increased from 3–45 g, the post-distributive half-life of thymidine elimination increased progressively

from 7–98 min. Zaharko et al. [117] suggested that renal secretion of thymidine is partially saturated at millimolar concentrations, because of their findings that the renal clearance of thymidine is only slightly greater than creatinine clearance at high doses of thymidine but almost four times greater than creatinine clearance at low doses of thymidine [34]. Thymidine is metabolized by the liver and other tissues [117]. Ensminger and Frei [35], using direct infusion of thymidine into the hepatic artery, have shown that the hepatic extraction of thymidine decreases from a maximum of 99% at 8 g/m^2 per 24 h to a minimum of 54% at 32 g/m^2 per 24 h.

Conventional Dose Chemotherapy

Dose-dependent pharmacokinetics have been shown for other anticancer drugs administered over more limited ranges of dose. An early example is a report by Fujita [43] that mitomycin C is cleared more rapidly after low doses than after high doses. The plasma half-life of mitomycin C calculated from Fujita's data is less than 6 min after a total dose of 2 mg and more than 20 min after a total dose of 30 mg. Mitomycin C is metabolically activated in vivo [63] and is cleared from the plasma primarily by metabolism [43]. Changes in metabolism of mitomycin C dependent upon dose could affect the drugs toxicity and antitumor activity.

5-Fluorouracil (5-FU) also exhibits dose-dependent pharmacokinetics. An early report by Clarkson et al. [18] suggested that 5-FU administered by continuous IV infusion at 5 or $30 \text{ mg} \cdot \text{kg}^{-1} \cdot \text{day}^{-1}$ was subject to more metabolic degradation than 15 mg/kg administered as an IV bolus. More recently Garrett et al. [45] demonstrated a decrease in total-body clearance of 5-FU at a total dose of 1,000 mg compared with 500 mg. Ensminger et al. [36] found a decrease in total-body clearance of 5-FU and no change in hepatic clearance as the dose of 5-FU infused was increased from $5.6\text{--}22.4 \text{ mg} \cdot \text{kg}^{-1} \cdot \text{h}^{-1}$. Speyer et al. [103] reported pharmacokinetics for 5-FU administered IP. Their data indicated a decrease in total-body clearance of 5-FU at high doses. This was most marked in one patient in whom clearance declined from $4.1\text{--}0.9 \text{ l/min}$ as the IP concentration was increased from 5–8 mM. Cano et al. [14] reported a lower total-body clearance of 5-FU, 1.1 l/min , when 5-FU was administered as an IV bolus of 15 mg/kg than when the same dose was infused over several hours, when the total-body clearance was 27.1 l/min . These authors reported a flow-limited model for the elimination of 5-FU based on the assumption of modulation of 5-FU metabolism

by pool size of dihydro-5-fluorouracil (5-FUH₂). The first and rate-limiting step in the catabolism of 5-FU is reduction to 5-FUH₂ [82]. Inhibition of the enzyme catalyzing this reduction, dihydrouacil dehydrogenase, has been reported to potentiate toxicity and antitumor activity in animals [23]. Collins et al. [22] have recently proposed a physiological pharmacokinetic model for 5-FU incorporating a saturable term for whole-body clearance (which includes metabolism and renal secretion) with a calculated K_m of 15 μM .

Adriamycin might exhibit dose-dependent pharmacokinetics. Mathematical models for adriamycin distribution have generally assumed linear pharmacokinetics [16, 54, 97]. The liver is the primary site for elimination of adriamycin, and over the narrow dose range of 30–40 mg/m², there is no alteration in hepatic extraction of adriamycin infused into the hepatic artery [44]. Creasey et al. [24], however, have reported that closely spaced IV doses of adriamycin, 15 mg/m² every 8 h, are associated with increased toxicity and higher plasma concentrations of adriamycin and metabolites after the sixth compared with the first dose. Their data also show a longer terminal half-life after a single IV dose of 90 mg/m² than after 22.5 mg/m². Gercovich et al. [47] reported a terminal half-life of 39 h for adriamycin following 60 mg/m² infused over 10 h, compared with a half-life of 27 h for the same dose given as a rapid infusion. Dose-dependent pharmacokinetics are not apparent in the results of a study by Bachur et al. [5], when adriamycin was administered at doses of 15–60 mg/m².

Arabinosyl-cytosine (AraC) is an anticancer drug that undergoes extensive deamination to form arabinosyl-uridine (AraU) [40]. The K_m of AraC for deaminase in human liver is $1.4 \times 10^{-4} M$ [13], which is similar to, or below the plasma concentration of AraC following doses of 100 mg/kg [31, 111]. Dedrick et al. [31] incorporated a term for saturable (Michaelis-Menten) metabolism in a physiological pharmacokinetic model for AraC. Their limited experimental data in patients receiving 1.2 and 8.6 mg AraC/kg suggest that the plasma concentration of AraC increases out of proportion to the increase in dose, raising the possibility that the deaminase is saturated at high doses of AraC.

3-Deazauridine (3-DAU) presents an interesting example of an anticancer drug whose removal appears to increase as the plasma concentration increases. Creaven et al. [27] presented data suggesting that the plasma half-life of 3-DAU decreased from 11 h to about 4 h as the total dose of 3-DAU was increased from 10 mg to 1500 mg. Benvenuto et al. [8] noted that the plasma pharmacokinetics of 3-DAU

were dependent upon its rate of infusion. After rapid (15–30 min) infusion of 3-DAU at doses between 1.5 and 5.3 g/m², the half-life of plasma elimination was 4.4 h. Following 5 days of continuous infusion of 3-DAU at 1.0–3.0 g/m² per day the half-life of plasma elimination was 21.3 h. A decrease in plasma half-life of 3-DAU with increasing dose has been reported in mice [29].

It is probable that cis-dichlorodiammineplatinum (CDDP) exhibits dose-dependent pharmacokinetics. Hall et al. [53] reported that the terminal half-life for elimination of total plasma CDDP was between 17.3 and 34.7 h following continuous infusion of CDDP at 20 mg/m² for 5 days. Gormley et al. [51] reported a half-life of plasma elimination of CDDP of 57 h following a 1-h infusion of CDDP at 40 mg/m². In contrast, DeConti et al. [30] found no differences in pharmacokinetic parameters of radioactively labeled CDDP at doses between 0.07 and 3.1 mg/kg administered as an IV bolus. The initial half-life ranged from 25.5–49.0 min and was followed by a slower half-life ranging from 58.0–73 h. CDDP is bound extensively to protein. Patton et al. [88] measured plasma concentrations of filterable (free) CDDP after slow and rapid IV administration. They reported a significantly shorter half-life, 26 min versus 44 min, and increased urinary excretion, 75% versus 49%, after CDDP at 100 mg/m² by 6-h infusion than after the same dose given as an IV bolus. The same group found no differences in the pharmacokinetic parameters of total CDDP and free CDDP when CDDP was administered as an IV bolus at a dose of 50 mg/m² [7].

Clinical Trials of New Anticancer Drugs

Clinical phase I trials involve planned dose escalations of new anticancer agents to determine the maximum tolerable dose in humans. As doses are increased pharmacokinetic parameters may change in a manner that affects drug toxicity. Work in our laboratory has shown a decrease in total body clearance of a new investigational anticancer drug L-2-amino-3-(N-hydroxy,N-nitrosamino)propionic acid (L-alanosine) as the dose is escalated [92] (Table 1). L-alanosine, an amino acid analogue, is extensively metabolized in humans. Less than 6% of the total dose is excreted unchanged in the urine in 24 h [92]. The major pathway for metabolism of L-alanosine in animals is transamination [66]. We have found evidence suggesting that transamination occurs in humans (G. Powis, 1981, unpublished observations). It is possible that the decreased clearance of L-alanosine at high doses results from saturation of the transamination pathway. We have

Table 1. Plasma clearance (Cl) of L-alanosine

	Dose (mg/m ²)					
	250	375	500	800	1,200	1,500
Cl (ml · min ⁻¹ · kg ⁻¹)	24.5	33.3	12.2	13.9	5.2	6.8

L-alanosine was administered to groups of three patients at the doses shown, over 10 min or for the 1,200 and 1,500 mg/m² dose levels, over 30 min

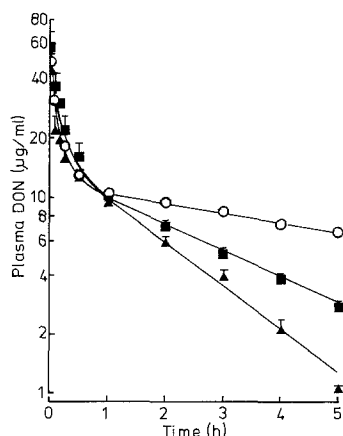


Fig. 1. Plasma levels of DON following IV administration of DON at doses of \blacktriangle , 300 mg/m² (three patients); \blacksquare , 450 mg/m² (three patients); and \circ , 550 mg/m² (one patient). Further patients could not be studied at the highest dose level because of unacceptable toxicity. Bars represent SEM. The continuous lines are computer fits to the data

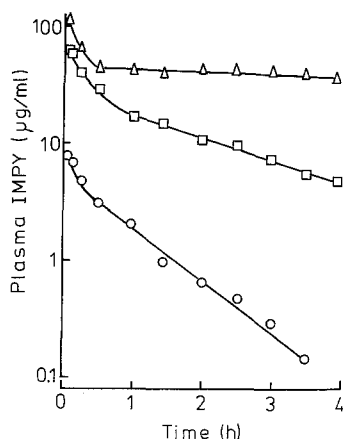


Fig. 2. Plasma levels of IMPY in rabbits following rapid IV administration of IMPY: \circ , 5 mg/kg; \square , 25 mg/kg; and \triangle 150 mg/kg. From Ames et al. [2]

also studied another amino acid analogue, 6-diazo-5-oxo-L-norleucine (DON), in a phase I clinical trial. DON is extensively metabolized in humans, with little or no unchanged drug appearing in the urine [91, 93]. Removal of DON from plasma is

dependent on the dose (Fig. 1). Although limited, the data are compatible with a dose-dependent memory effect such as that produced by metabolite inhibition of biotransformation of parent compound. Confirmation of this hypothesis will require identification of metabolic products of DON and the demonstration that they inhibit metabolism. A drug we have studied in animals, although not in man, is 2,3-dihydro-1-H-imidazol[1,2B]pyrazole (IMPY). Removal of IMPY from plasma in the rabbit is dose-dependent (Fig. 2). The half-life of plasma IMPY is 45 min at a dose of 5 mg/kg and 640 min at 150 mg/kg administered as an IV bolus [2]. Dose dependency has been reported in humans by Staubus et al. [104], with a more prolonged terminal half-life at higher doses. This might explain the sudden onset of serious toxicity reported for IMPY as the dose is escalated [83].

There is limited evidence that the pharmacokinetics of other anticancer drugs exhibit dose dependency, including 5-azacytidine [62] and 6-mercaptopurine [76]. The blood levels and half-life of spirogermanium have been reported to increase considerably after repeated daily administration [71]. ICRF-159 exhibits dose-dependent absorption, with less drug absorbed when administered as a single oral dose of 3 g/m² than when the same total dose is divided into three equal portions and administered orally every 6 h [26]. 2-Amino-1,3,4-thiadazole is an experimental anticancer agent, which exhibits dose-dependent pharmacokinetics due to saturation of metabolism in dogs and monkeys [33, 68]. A decreased urinary excretion of N-(phosphonacetyl)-L-aspartic acid (PALA) has been reported in mice by Chadwick et al. [15], which was suggested to be due to saturation of binding sites for PALA, possibly in bone. Studies in humans, however, have shown no convincing evidence for dose-dependent PALA pharmacokinetics [37, 77].

Not all anticancer drugs given in relatively high doses exhibit dose-dependent pharmacokinetics. For example, cyclophosphamide has been administered over a wide range of doses, 1–80 mg/kg. The major pathway for cyclophosphamide elimination is hepatic metabolism [110]. The *K_m* for hepatic metabolism is over 1 mM [21, 102], which is considerably in excess of plasma concentrations even at high doses [65] and probably accounts for the fact that cyclophosphamide does not show dose-dependent pharmacokinetics [52].

It should also be emphasized that the pharmacokinetic behavior of one drug may be profoundly altered by the presence of other drugs. A striking example is the effect of thymidine upon the plasma elimination and urinary excretion of 5-FU. Wood-

cock et al. [116] reported that administration of thymidine to humans at 7.5 g increased the plasma half-life of 5-FU from 6–135 min and that 15 g thymidine increased the plasma half-life to 188 min. They provided evidence that thymidine all but eliminates oxidative metabolism of 5-FU, resulting in renal clearance becoming the primary route of elimination of 5-FU in the presence of thymidine, as against elimination by metabolism when 5-FU is administered alone. This phenomenon is akin to decreases seen in elimination of parent drug secondary to inhibition of metabolizing enzymes by metabolite of the parent drug, in that thymine, a metabolite of thymidine, competes with 5-FU for catabolic enzymes.

Consequences of Dose-dependent Pharmacokinetics

Several recent studies suggest that for some anticancer drugs known to exhibit dose-dependent pharmacokinetics saturation of elimination and/or uptake plays an important role in determining the occurrence of drug toxicity [24, 26, 47, 85, 103, 106] and, more provocatively, the occurrence of therapeutic effect [14, 56, 112]. Current approaches to cancer chemotherapy present unique opportunities to study the pharmacokinetic behavior of foreign compounds of widely differing chemical structure, because of the range of drug concentrations routinely used to establish the maximal tolerable dose in the early stages of drug development. We anticipate that as methods for 'rescuing' patients from unacceptable drug toxicity are improved, there will be an increasing trend to use very high-dose therapy to enhance entry of drugs into resistant cells and into pharmacological sanctuaries. As wider ranges of drug doses are studied it is to be expected that dose-dependent pharmacokinetic behavior of many anticancer drugs will be noted and will receive detailed study.

Such information may permit rational design of regimens that minimize toxicity and maximize therapeutic effect. Several examples have been provided of drugs whose metabolism and pharmacokinetic parameters change considerably depending on whether the dose is given by IV bolus or as an infusion. Increasingly anticancer drugs are being given in very large doses. Methotrexate was the first drug to be used at very high doses to maximize entry into tumor cells [11] and into tumor sanctuaries such as the central nervous system [101]. Thymidine is being given in high doses to achieve cytotoxic concentrations in the blood [117] and to modulate the metabolism of other cytotoxic agents [116]. It is probable that soon other drugs will be given in much

higher doses than are currently used as new techniques, such as IP administration [103], transplantation of heterologous bone marrow [107] or autologous bone marrow [109], and rescue with specific pharmacologic agents, are more fully developed.

The application of pharmacokinetic principles to the improvement of cancer chemotherapy is in an early stage of development and will be pursued vigorously in the future [25, 38, 84]. In this review we have attempted to show that dose-dependent pharmacokinetic behavior of anticancer drugs is likely to be of special relevance to the development of more effective therapeutic regimens.

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